Use of argon plasma to enhance soft-tissue integration of prosthetic components: a randomized, controlled animal study

Abstract

Objective

This paper aimed to assess histologically the soft- and hard-tissue changes after insertion of cleaned and activated titanium implant abutments.

Methods

Three months after tooth extractions, four implants were inserted in one side of the mandible. Before connecting the abutments to the implants, two of them were detoxified (test group), while two were left untreated (control group). The abutments were randomly placed on the two distally or on the two mesially located implants. After one month, the same procedure was repeated on the other side of the mandible. The animals were euthanized one month after the last surgery. Histological analysis was performed to identify the shoulder of the implant, the most coronal bone-to-implant contact, the top of the adjacent bony crest, the top of the periimplant mucosa (PM) and the apical termination of the junctional epithelium (AJE).

Results

All of the animals remained in good health during the experimental period. No statistically significant differences were found between the test and control sites (p > 0.05). Between the first and the second time points, no statistically significant differences between the groups were found, except for PM–AJE of the test group, with higher values observed two months after implant placement. However, a trend of better marginal bone levels was found in the test group, compared with the control group, at the second time point.

Conclusion

Although differences between the test and control groups failed to reach significance, a trend of better marginal bone levels was found at the test sites compared with the control sites.

Keywords

Argon plasma, soft-tissue adhesion, animal study, titanium abutment.
Introduction

Periimplant soft- and hard-tissue stability is critical for the success of an implant-supported restoration, from a functional and esthetic point of view. It has been described that the relationship between the implant–abutment connection and surrounding hard and soft tissue plays an important role in establishing such mechanical and biological stability. In fact, the literature has demonstrated that, when an implant is exposed to the oral environment after the connection of a prosthetic component, periimplant hard-tissue level changes may occur and that the amount of bone remodeling, characterized by circumferential (horizontal and vertical) bone loss, should remain stable after one year. Several factors and, in particular, disruptions occurring after prosthetic connections may affect periimplant resorption, since the bacterial contamination of the implant–abutment junction from the oral cavity has been shown to trigger a hard-tissue response.

Many strategies have been advocated to minimize the effect of this contamination clinically: mechanical improvement of the implant–abutment connection stability, implant–abutment microgap shifting from the vital bone, and reducing the number of abutment dis- and reconnections. Nevertheless, minimal bone resorption (0.5 mm) has been observed in longitudinal analysis.

Bone resorption might be related to the contaminants (bacteria, wear microparticles and pollution from laboratory procedures) present on the abutment at the time of implant–abutment connection. In fact, the presence of contaminants on the abutment surface can still be observed after the steam cleaning protocol after technical laboratory procedures. Since the abutment comes into contact with both bone and connective tissue, abutment cleanliness appears to be important. In fact, the presence of contaminants at the platform–abutment level has been suggested to cause associated tissue-damaging inflammation. Titanium wear microparticles have been demonstrated to activate osteoclastogenesis. Additionally, it has been shown how interactions between cellular components and implant–abutment materials influence the healing process around implants and how these interactions are regulated by the state of the surface.

In order to protect abutments against such pollutants, plasma cleaning of customized abutments has recently been advocated. Plasma cleaning has been demonstrated in vitro to have a triple effect on titanium: cleaning, corrosion protection and increased surface energy. However, there is a lack of evidence in the literature regarding the clinical relevance of a plasma cleaning procedure performed on dental implant abutments.

Although there are certain differences in the inflammatory response and in the bacterial population, the beagle dog model has been extensively used in experimental study because of its size and its extremely cooperative nature. Although some major differences exist between dogs and humans, all periodontal tissues and the size of the teeth are quite similar to those observed in humans. Furthermore, they are a very inbred type of animal with very limited anatomical differences between the various dogs. The aim of this animal study was to assess histologically soft- and hard-tissue adaptation after insertion of cleaned and activated titanium implant abutments. The null hypothesis was that argon plasma cleaning treatment of abutments does not have any positive or detrimental effect on periimplant bone remodeling and soft-tissue adhesion.

Materials and methods

Subjects

This study followed the ARRIVE guidelines. The research protocol was approved by the local ethics committee for animal research at the University of São Paulo, Ribeirão Preto, Brazil. Eight beagle dogs were used for the experiment. The animals were pre-anesthetized for all surgical procedures with Acepran 0.2% (0.05 mg/kg; Univet-vetnil, São Paulo, Brazil) and sedated with Zoletil (10 mg/kg; Virbac, St. Louis, Mo. U.S.), and the maintenance of the anesthesia was performed with inhalation of Forane (Baxter Hospitalar, São Paulo, Brazil).

All mandibular premolars and the first molars were extracted bilaterally and after three months, a crestal incision was performed in the premolar–molar region of one randomly selected side of the mandible. Full-thickness mucoperiosteal flaps were elevated, and four experimental sites were selected in the edentulous alveolar ridges of the mandible, two in the anterior and two in the distal regions. The surgical preparation of the sites was performed accord-
Twist drills were used to prepare each recipient site. Four implants (Premium, Sweden & Martina, Due Carrare, Italy), 7 mm long and 3.3 mm wide, were subsequently inserted. Before connection, two of the four abutments were detoxified (test group), while two were left untreated (control group). One abutment of each group was placed on to one of the two mesially and one of the two distally located implants, respectively, according to the randomization allocation. The flaps were sutured to allow nonsubmerged healing. After one month of healing, the surgical procedures were applied on the other side of the mandible, again following a randomization protocol.

After every surgery, the animals underwent antibiotic treatment for ten days (Stomorgyl 10, one tablet/10 kg daily; Merial Saúde Animal, Paulinia, Brazil) and received anti-inflammatory drugs for five days (Maxicam 2 mg, one tablet/10 kg daily).

Fig. 1
Ground section illustrating the results of healing after one month at a test site. 16× magnification. Alizarin red and Stevenel’s blue stain.

Fig. 2
Ground section illustrating the results of healing after one month at a control site. 16× magnification. Alizarin red and Stevenel’s blue stain.
Abutment preparation

The control group abutments, after being milled and polished, were cleaned by steam for 30 s...
Plasma effect on abutments (VAP 1; Zhermack, Cologne, Germany) before delivery. The test group abutments, after being milled, polished and cleaned for 30 s (VAP 1), underwent argon plasma treatment (75 W power and -10 MPa pressure for 12 min at room temperature) in a plasma reactor (Diener electronic, Jettingen, Germany) present in the same clinical facility, but in a different room.

**Histological preparation**

Individual bone blocks containing one implant each and the surrounding soft and hard tissue were fixed in a 4% formaldehyde solution. The blocks were dehydrated in a series of graded alcohol solutions and finally embedded in resin (LR White, hard grade; London Resin Company, Berkshire, U.K.). The blocks were cut in a buccolingual plane using a diamond band saw fitted in a precision slicing machine (EXAKT Apparatebau, Norderstedt, Germany) and then reduced to a thickness of about 50–60 μm using a cutting–grinding device (EXAKT Apparatebau). The histological slides were stained with alizarin red and Stevenel’s blue and examined under a standard light microscope for histometric analysis.

**Histological analysis**

In a microscope at 100× magnification, the following landmarks were identified: the shoulder of the implant (IS), the most coronal bone-to-implant contact (B), the top of the adjacent bone

<table>
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<tr>
<th><strong>Table 1</strong></th>
<th>Comparison between test and control groups one month after implant placement. Data are presented in mm as mean ± standard deviation (Median; IRG 25th–75th mm).</th>
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<tr>
<td><strong>n</strong></td>
<td><strong>IS-B</strong></td>
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<td><strong>Test</strong></td>
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<td><strong>Control</strong></td>
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<td><strong>Test</strong></td>
<td>8</td>
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<td><strong>Control</strong></td>
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<td><strong>p value</strong></td>
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<th><strong>Table 3</strong></th>
<th>Comparison between one and two months timepoints. Data are presented in mm.</th>
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<td><strong>n</strong></td>
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<td><strong>Test</strong></td>
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<td><strong>2 months</strong></td>
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<td><strong>Control</strong></td>
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<td><strong>p value</strong></td>
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crest (C), the top of the periimplant mucosa (PM) and the apical termination of the junctional epithelium (AJE). The following linear measurements were performed parallel to the long axis of the implant: the vertical distances between (i) IS and B (IS–B), (ii) IS and C (IS–C), (iii) PM and C (PM–C), and (iv) PM and AJE (PM–AJE).

**Randomization procedure**

The dogs randomly received implants in the right or left side of the mandible in the first surgery and in the other side in the next surgery. Immediately after implant placement, untreated (as they come from industry; control group) or detoxified abutments (argon plasma; test group) were randomly assigned to the implant sites. A balanced random permuted block approach was used to prepare the randomization tables to prevent an unequal balance between the two groups. A blinded statistician generated the allocation sequence and assigned abutments to sites. Assignment was performed using opaque envelopes containing the generated unique randomization code opened immediately after implant placement.

**Statistical analysis**

Mean values and standard deviations were calculated for each outcome variable. Measurements of the buccal and lingual aspects were performed, with an accuracy of 0.01 mm. Mean values between the buccal and lingual aspects were obtained.

Median and interquartile values were also calculated in order to give a better description of the data set (25th, 50th [median] and 75th percentiles). All measurements were rounded to the nearest decimal. Data were pooled for abutment treatment (cleaned or activated titanium implant abutments). The primary variables were IS–C and IS–B. Differences between the test and control sites were analyzed using the nonparametric Mann–Whitney U test. Comparisons between each time point were made by paired tests in order to detect any changes in marginal periimplant bone levels. All statistical comparisons were conducted at the 0.05 level of significance.

**Results**

In total, 64 implants were placed in eight beagle dogs. All of the animals remained in good health during the experimental period and no complications occurred during the healing period. An n = 8 was reached at the one-month period, while an n = 7 was reached at the two-month period because one dog lost implants in the control group.

After one month of healing (Table 1), in the test group, at the buccal aspect, IS–B was 1.43 ± 0.99 mm, IS–C was 0.67 ± 0.53 mm, PM–C was 2.61 ± 0.37 mm and PM–AJE was 2.39 ± 0.33 mm. In the control group, IS–B was 1.61 ± 0.74 mm, IS–C was 0.50 ± 0.59 mm, PM–C was 2.59 ± 0.36 mm and PM–AJE was 2.59 ± 0.41 mm. No statistically significant differences were found between the groups (p > 0.05; Table 1). The median and interquartile values are reported in Table 1.

After two months of healing (Table 2), in the test group, IS–B was 1.72 ± 0.70 mm, IS–C was 0.50 ± 0.48 mm, PM–C was 2.59 ± 0.27 mm and PM–AJE was 2.78 ± 0.44 mm. In the control group, IS–B was 2.18 ± 0.71 mm, IS–C was 0.91 ± 0.64 mm, PM–C was 2.86 ± 0.84 mm and PM–AJE was 2.42 ± 0.64 mm. No statistically significant differences were found between the groups (p > 0.05; Table 2). The median and interquartile values are reported in Table 2.

The results between the first and the second time points showed no statistically significant differences between the test and control groups, except for PM–AJE of the test group, with higher values observed two months after implant placement (Table 3).

**Discussion**

Although cleaning procedures (cleansing with alcohol, soap or steam vapor) at the end of the laboratory phase should be carried out according to law in the U.S.,21 Europe (EN ISO 17664:2004) and Australia (ADA’s Guidelines for Infection Control, 2015), several microscopic impurities can be detected on the abutment surface even after these treatments. Microscopic impurities on the abutment surface due to industrial processes can often be detected also after industrial prepackaging procedures.22 Additional metallic microparticles mixed with lubricant and oxide layers can be produced during the laboratory workflow and adsorbed contaminants can be accumulated during delivery.17 Such pollution and oxide layers can directly and indirectly trigger a soft- and hard-tissue inflammatory response or at least alter the interaction with the soft- and hard-tissue environments.15
A very important area of research is the development of efficient high-vacuum technologies able to clean and functionalize surfaces to replace conventional methods of cleaning metallic or polymeric surfaces. In this context, cold plasma technology represents an efficient alternative and has been the subject of increasing attention.

Low-temperature plasma equipment works within a vacuum chamber in which atmospheric gases have been evacuated typically below 0.1 torr. This low pressure allows for a relatively long free path of accelerated electrons and ions. Since the ions and neutral particles are at or near ambient temperatures and the electrons, which are at high-temperature or electronvolt levels, have relatively few collisions with molecules at this pressure, the reaction remains at low temperature. With appropriate plasma parameters, argon plasma removes all chemical traces of previous treatments, in effect producing cleaner and better controlled surfaces than with conventional preparation methods.23

Furthermore, the advantages of plasma cleaning can be exploited to enhance the soft-tissue response during the prosthetic implant phase. Change in the surface wettability of commercial pure titanium, in fact, might determine the functional response of fibroblasts and is therefore a critical factor for the adhesion of soft tissue to the titanium abutment.

In the present study, no differences were found between the test and control groups for the first time point (one month of healing). However, at the second time point (two months), despite the absence of statistically significant differences, a trend showing slightly better marginal bone levels in the test group, compared with the control group, was observed. This may explain why a previously published study showed statistically significantly better radiographic bone level maintenance in humans after two- and five-year follow-up at the treated sites.24 This may suggest that, in a longer follow-up, statistical significance could also be reached in experimental studies.

Although a recently published in vitro study presented no quantitative differences in terms of cell adhesion between plasma-cleaned or only sterilized titanium disks after 8 h, the same study reported qualitative differences in terms of cell spreading.25 This may suggest that a shorter analysis time frame may only show differences at the microscopical level.

It can be speculated that the differences in terms of IS–B, IS–C and PM–C between the test and control groups, although they did not reach significant levels, could be the early expression of better organization of perimplant soft tissue due to a more “proactive” abutment. This speculation could be supported by the dissimilar outcomes reported by two studies with different time points. In fact, while Canullo et al. reported an absence of histological differences after one week,26 Garcia et al. observed significantly better outcomes after two weeks in terms of connective cell adhesion and soft-tissue arrangement around abutments cleaned by plasma compared with sterile abutments.27 For this reason, the outcomes of the present investigation should be taken with caution owing to the short follow-up that may have failed to disclose differences.

Conclusion

Within the limitations of the present study, although differences between the test and control groups failed to reach significance, a trend of better marginal bone levels was found at the test sites compared with the control sites. This might suggest that the use of argon plasma might improve the soft-tissue integration of titanium abutments.

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Competing interests

The authors declare that they have no competing interests.
Plasma effect on abutments

References


